

Interpreting Impedance Images ... *Interesting or Irrelevant?*

MIRAN Workshop, U. Manchester, UK:
Chest EIT: Vision, Status & Priorities
16 November 2012

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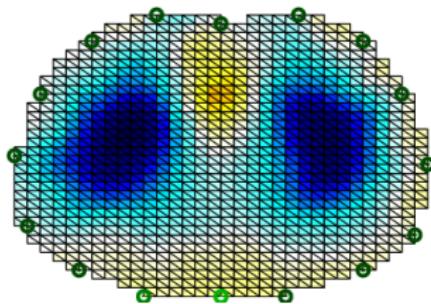
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EIT Images: *Interesting or Irrelevant?*

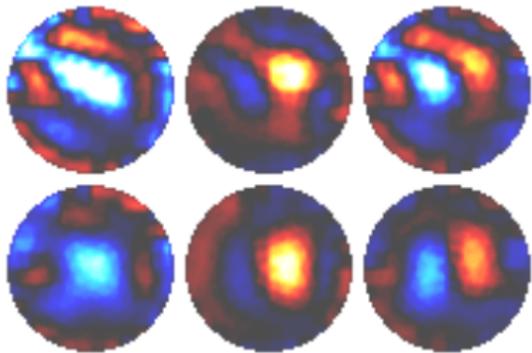
- Motivating Question:
What do we need from the engineers?
- Recent advances
- Requirements for clinical EIT
 - current work to address them
- What should be our priorities?

Recent Advances

GREIT

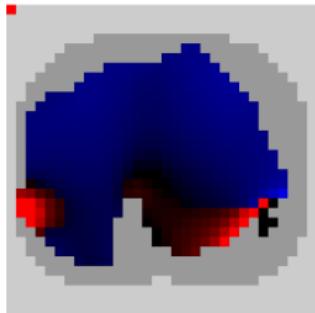


Electrode Errors

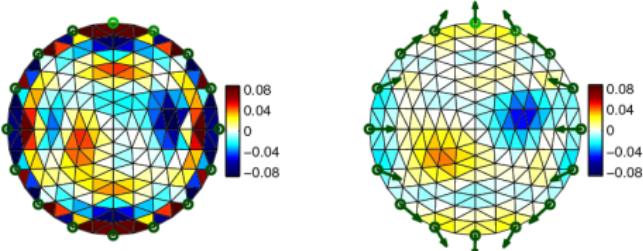


Lung Parameters

Alveolar Collapse (red): 2%
Alveolar Overdistension (blue): 37%
PEEP: 16 cm H₂O



Electrode Movement



Requirements for clinical EIT

From “Whither EIT” *Phys. Meas.* (2012)

- Availability of EIT devices
- Standards
- Robustness
- Useful software
- Useful parameters
- Standardized procedures

Requirements: *availability*

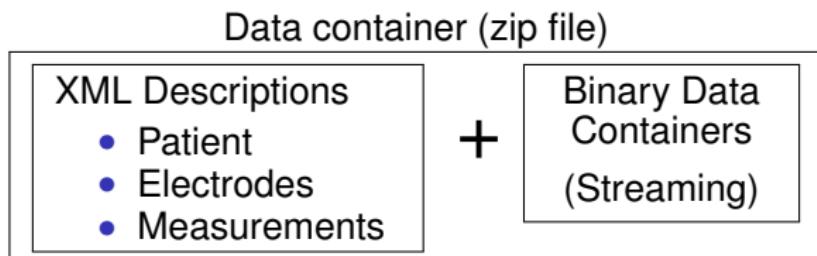
*EIT devices must be readily available at a reasonable cost.
Since EIT uses components common to consumer electronics,
increases in volume should strongly reduce costs.*

- Some progress
- Still a big problem

Requirements: *standard formats*

*EIT data and images must be accessible in standard formats.
For images, the natural format is a DICOM class.*

- It's not hard to do a DICOM class for EIT
- Work on a data format

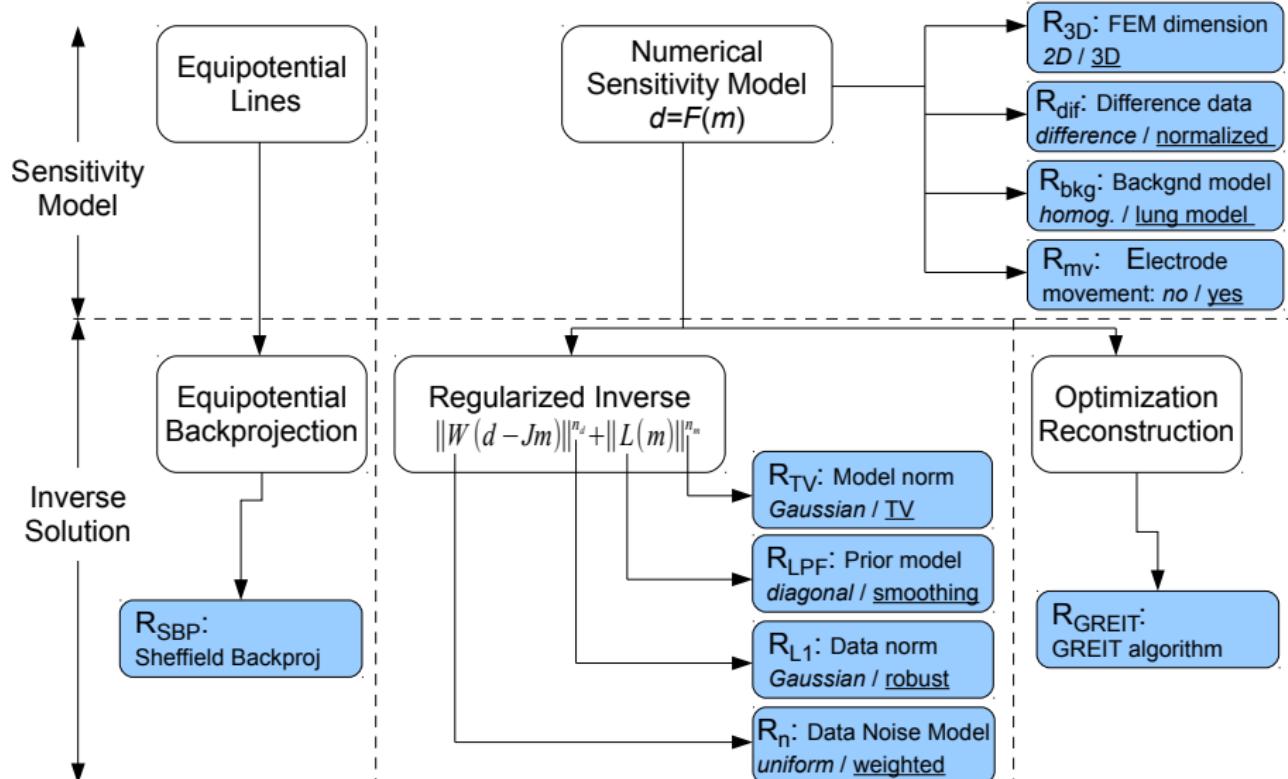


Requirements: *robustness*:

EIT systems must be robust against electrode contact problems and electrical interference. Systems must automatically compensate (if possible) for electrode errors or give appropriate warnings.

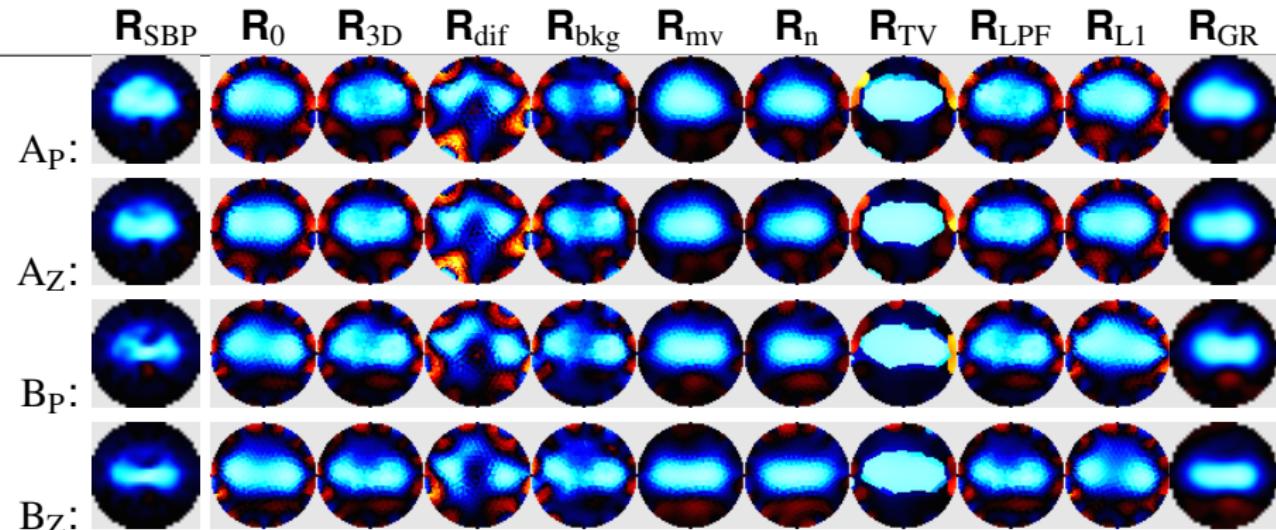
- Algorithm Evaluations
- Electrode error compensation
- Data quality measures
- Robust Algorithms

robustness: Algorithm Evaluations



Taxonomy of direct EIT reconstruction algorithms, classified in terms of the selection of forward and inverse model parameters.

robustness: Algorithm Evaluations



EIT images for all algorithms from two animals (A&B). For each animal, images of V_T at PEEP (\cdot_P) and ZEEP (\cdot_Z) are shown individually normalized to the maximum amplitude in each image (Blue: decrease in conductivity, Red: increase in conductivity).

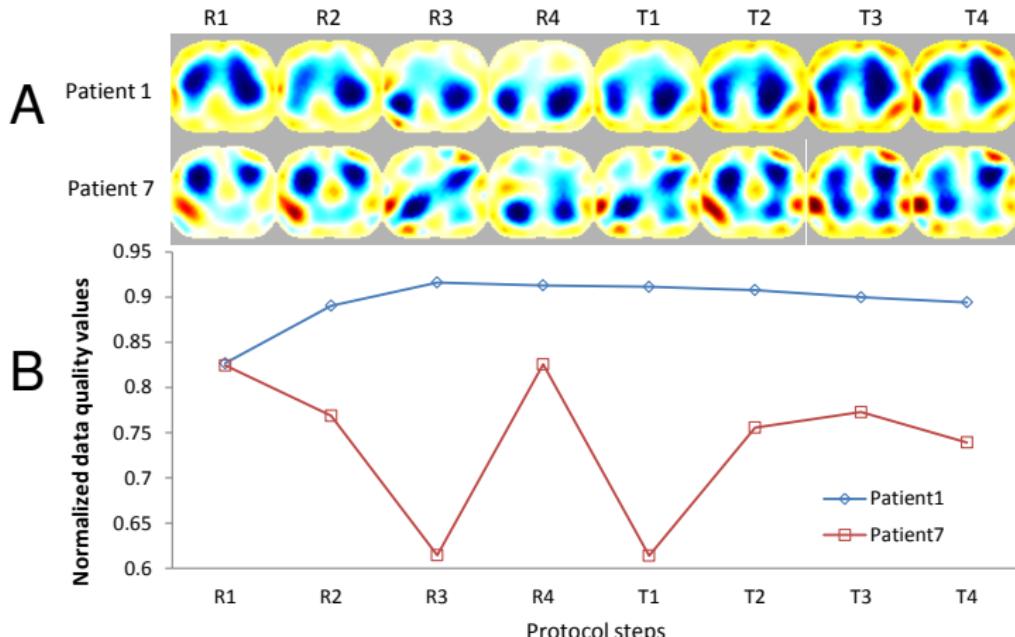
robustness: Algorithm Evaluations

Performance of different image reconstruction algorithms during mechanical ventilation with constant tidal volume and variable end-expiratory pressure and O₂ fraction – detection of global and regional tidal and end-expiratory lung volumes

| Expected finding | R _{SBP} | R ₀ | R _{3D} | R _{dif} | R _{bkg} | R _{mv} | R _n | R _{TV} | R _{LPF} | R _{L1} | R _{GR} |
|--|------------------|----------------|-----------------|------------------|------------------|-----------------|----------------|-----------------|------------------|-----------------|-----------------|
| V _T is independent of PEEP | | | | | | | | | | | |
| V _{T,E,Z,21} = V _{T,E,P,21} | 0.021* | 0.332 | 0.175 | 0.203 | 0.387 | 0.014* | 0.001* | 0.845 | 0.172 | 0.000* | 0.006* |
| V _{T,E,Z,100} = V _{T,E,P,100} | 0.009* | 0.041* | 0.027* | 0.052 | 0.062 | 0.008* | 0.009* | 0.208 | 0.027* | 0.001* | 0.008* |
| V _T is independent of F _I O ₂ | | | | | | | | | | | |
| V _{T,E,Z,21} = V _{T,E,Z,100} | 0.031* | 0.015* | 0.018* | 0.001* | 0.008* | 0.044* | 0.035* | 0.111 | 0.017* | 0.000* | 0.041* |
| V _{T,E,P,21} = V _{T,E,P,100} | 0.003* | 0.007* | 0.006* | 0.026* | 0.009* | 0.003* | 0.001* | 0.134 | 0.005* | 0.000* | 0.002* |
| V _T is reproducible | | | | | | | | | | | |
| V _{T,E,Z1} = V _{T,E,Z2} | 0.002* | 0.006* | 0.004* | 0.000* | 0.003* | 0.003* | 0.001* | 0.018* | 0.004* | 0.001* | 0.002* |
| V _{T,E,P1} = V _{T,E,P2} | 0.000* | 0.000* | 0.000* | 0.001* | 0.000* | 0.000* | 0.000* | 0.002* | 0.000* | 0.000* | 0.000* |
| CoG is PEEP dependent | | | | | | | | | | | |
| CoG _{E,Z,21} > CoG _{E,P,21} | 0.069 | 0.097 | 0.094 | 0.156 | 0.138 | 0.064 | 0.050 | 0.090 | 0.094 | 0.138 | 0.051 |
| CoG _{E,Z,100} > CoG _{E,P,100} | 0.024* | 0.032* | 0.032* | 0.049* | 0.045* | 0.025* | 0.022* | 0.030* | 0.032* | 0.056 | 0.022* |
| CoG is F _I O ₂ dependent | | | | | | | | | | | |
| CoG _{E,Z,21} < CoG _{E,Z,100} | 0.006* | 0.007* | 0.006* | 0.015* | 0.010* | 0.006* | 0.006* | 0.007* | 0.006* | 0.014* | 0.006* |
| CoG _{E,P,21} < CoG _{E,P,100} | 0.552 | 0.526 | 0.529 | 0.458 | 0.539 | 0.526 | 0.581 | 0.556 | 0.528 | 0.493 | 0.530 |
| CoG is reproducible | | | | | | | | | | | |
| CoG _{E,Z1} = CoG _{E,Z2} | 0.007* | 0.016* | 0.020* | 0.192 | 0.017* | 0.039* | 0.010* | 0.017* | 0.018* | 0.008* | 0.017* |
| CoG _{E,P1} = CoG _{E,P2} | 0.001* | 0.001* | 0.002* | 0.002* | 0.001* | 0.008* | 0.006* | 0.002* | 0.002* | 0.000* | 0.007* |

E, Measures by EIT; V_T, tidal volume; PEEP (P), positive end-expiratory pressure; ZEEP (Z), zero end-expiratory pressure; F_IO₂, fraction of O₂ in inspired gas; 21, F_IO₂ equal to 21%; 100, F_IO₂ equal to 100%; indices 1 and 2 identify the first and the second measurements at identical ZEEP or PEEP levels; Up, upper or nondependent lung regions; Lo, dependent lung regions

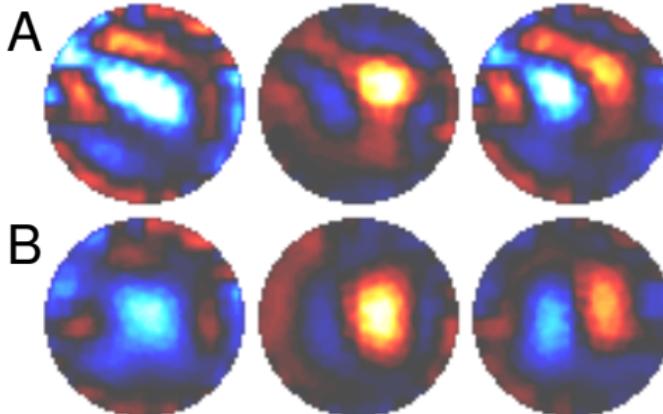
robustness: Data quality measures



Clinical data and data quality metric for each stage of the protocol (R1–R4 — recruitment: PEEP↑, T1–T4 — titration: PEEP↓).
A: EIT images (one-step Gauss-Newton solver with a 2D forward model), B: Calculated data quality.

robustness: Electrode error compensation

- Offline compensation using “jack-knife” approach (2005)



EIT images in anaesthetised, ventilated dog

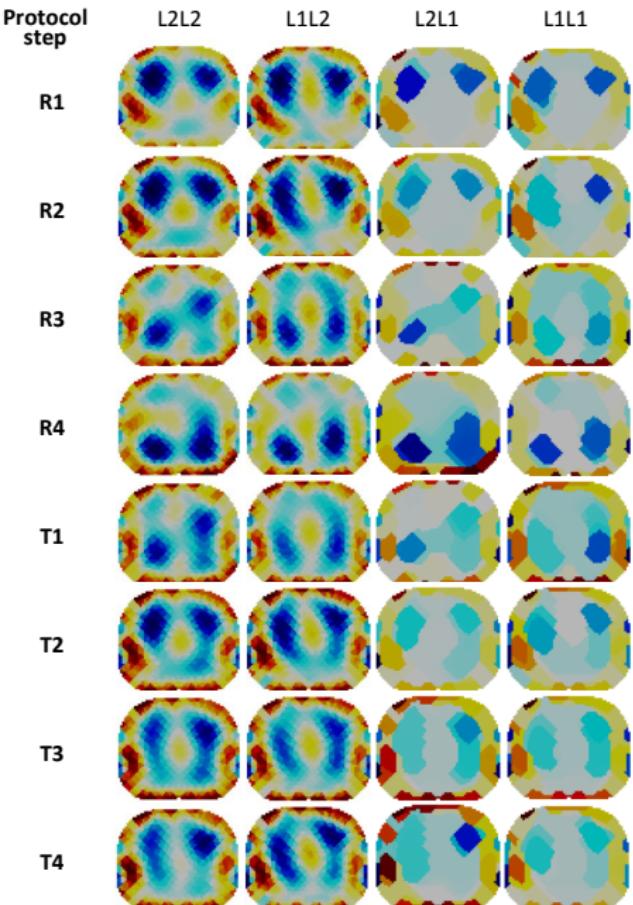
A: uncompensated, *B:* compensated. *Left:* ventilation *Centre:* saline (right lung) *Right:* ventilation and saline

- Automatic detection (via reciprocity comparison) (2009)
- New work to speed online calculation & use data quality

robustness: Robust Algorithms

- ℓ_1 norm for the image prior allows “blocky” reconstructions
- ℓ_1 norm for the data mismatch gives improved robustness to outliers

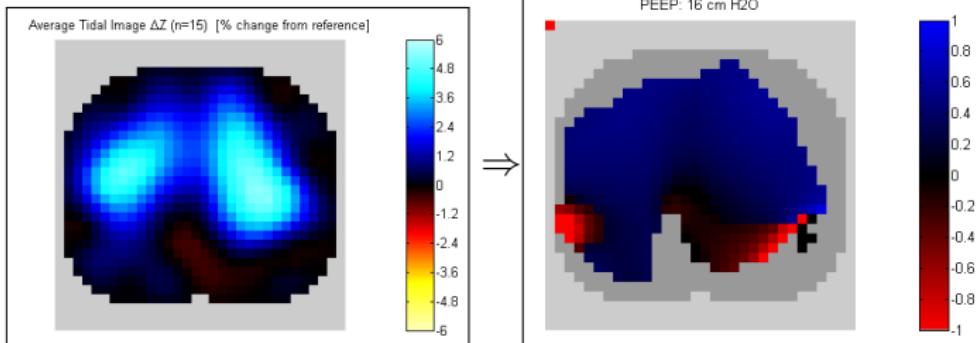
Figure: Reconstructions with mixed (data/image) norms for clinical data for each stage of the protocol (R1–R4 — recruitment: PEEP \uparrow , T1–T4 — titration: PEEP \downarrow).



Requirements: *useful software*:

Software must have an intuitive interface focused on the clinical user. EIT parameters should relate to those commonly used: pressures, volumes, time, or fractions (not ΔZ). Analysis must be on-line (not retrospective).

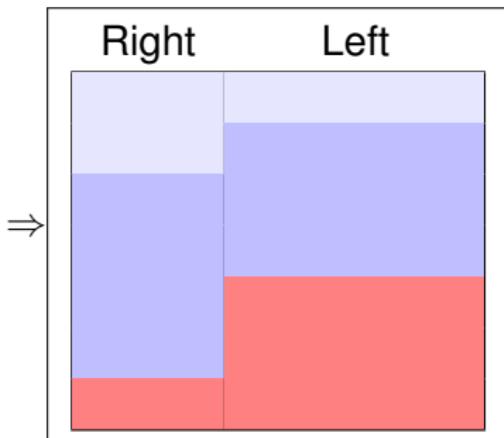
- Agreement that we need *overdistention* and *collapse* fractions.



Requirements: *standardized procedures:*

Standardize EIT protocols (e.g. duration of PEEP steps, magnitude of steps, type of ventilation, EIT frame rates, additional measurements). . . automated approaches for data analysis and interpretation should be included.

- Which information from EIT impacts care?
How to present information?



Thoughts (from “Whither EIT”)

- EIT is at a critical time.
 - a large and growing clinical interest
 - commercial devices on the market.
- Risk: enthusiasm dissipates, as new clinical researchers unable to reliably use EIT,
 - unable to usefully interpret the images generated
 - images ruined by errors.
- Is EIT “another technology too complicated for the clinic”?

So, we need good advice (for beginners) on how to

- conduct
- analyse

simple EIT experiments/clinical protocols

Concept for Graphical Analysis tool (*View Screen*)

View

File Edit Subject Tools Help



Subject: Control
Subject #: 1
Phase (A) : $t = -1\text{h}$ angle = -45°

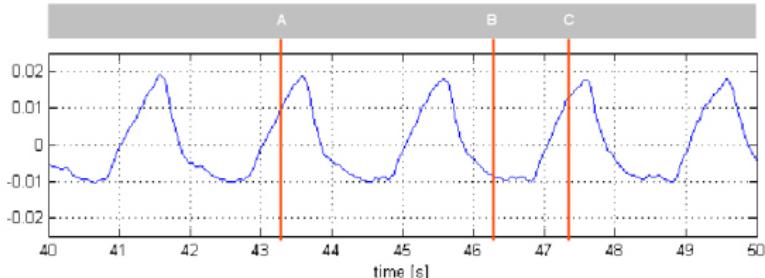
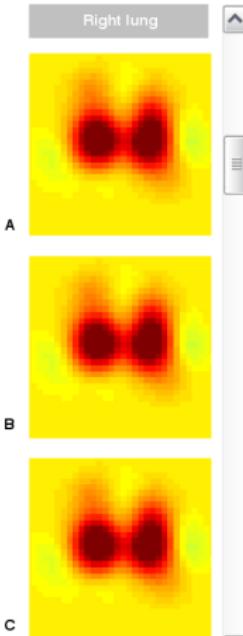
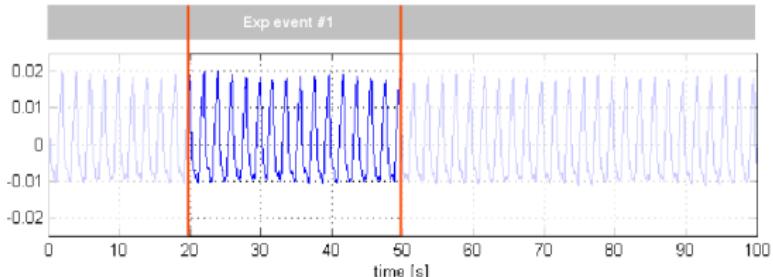
data

view

eval

Researcher
Researcher Information

Look
Dynamic
Static
Label
Left Lung
Right Lung
Sync



Concept for Graphical Analysis tool (*Eval Screen*)

Evaluate



File Edit Subject Tools Help



Subject: Control
Subject #: 1

data view eval

Researcher Researcher information

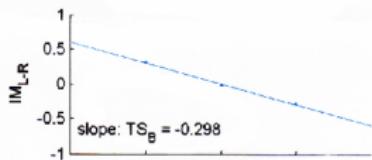
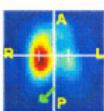
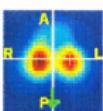
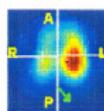
Evaluate

Design

B: Left

B: Horizontal

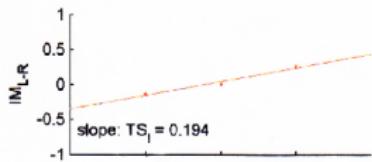
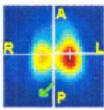
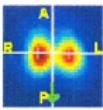
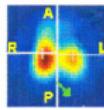
B: Right



I: Left

I: Horizontal

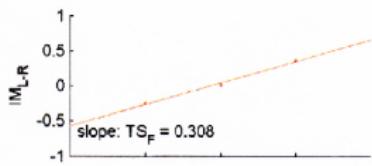
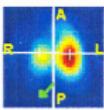
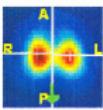
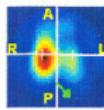
I: Right



F: Left

F: Horizontal

F: Right



Recommendations: “Whither EIT”

- think about the physiology;
 - e.g. EIT measure “my patient’s lungs are 30% collapsed” provides insights which lead to interventions
- analyze EIT images in creative ways
 - exploit the parameter “time” and many of sophisticated signal processing algorithms to generate new parameters.
- To solve these problems, we must work in *interdisciplinary teams* (clinical, engineering and mathematical experts).

Requirements: collaboration

EIDORS ⇒ ...

Sharing Code

The screenshot shows the EIDORS software interface. On the left, a sidebar lists various links such as Main, Documentation, Tutorials, Applications, FEM Modeling, GREIT, Old tutorials, Download, Contrib Data, GREIT, Browse Docs, and Browse SVN. The main window title is "EIDORS: Electrical Impedance Tomography and Diffuse Optical Tomography Reconstruction Software". Below the title, there is a section titled "Using Netgen to create elliptical EIDORS Models". It contains text explaining that EIDORS can use Netgen to create 2D and 3D models, followed by a code snippet:

```
fmdl= ng_mk_ellip_models([1,1.5,0.8],[0],[ ]); show_fem(fmdl);
```

. To the right of the code is a 3D visualization of a semi-elliptical volume mesh. A coordinate system is shown with values 1, 0.8, and n.a.

Sharing Data

The screenshot shows a web browser window titled "EIDORS" displaying a page from "eidors3d.sourceforge.net". The URL is "eidors3d.sourceforge.net/data_contrib/lf-neonate-spontaneous/index.php". The page is titled "Contributed EIT Data:". It contains the following information:

| Authors: | S. Heinrich, H. Schifmann, A. Freirichs, A. Klockgether-Radke, I. Freirichs |
|--------------------------------------|--|
| Date: | 2006 |
| Brief Description: | 10-day old spontaneously breathing neonate lying in the prone position with the head turned to left. Data were published in S. Heinrich, H. Schifmann, A. Freirichs, A. Klockgether-Radke, I. Freirichs, Body and head position effects on regional lung ventilation in infants: an electrical impedance tomography study , Intensive Care Med., 32:1392-1398, 2006. |
| License: | Creative Commons Artistic License (with Attribution) |
| Attribution Requirement: | Use or presentation of these data must acknowledge Inéz Freirichs, and reference this publication: S. Heinrich, H. Schifmann, A. Freirichs, A. Klockgether-Radke, I. Freirichs, Body and head position effects on regional lung ventilation in infants: an electrical impedance tomography study , Intensive Care Med., 32:1392-1398, 2006. |
| Format: | EIT data were acquired with the Göttingen Goe-MF II device, 220 frames, 13 frames/s. Data are .GET file format. |
| Methods: | Neonate in prone position, with electrode #1 at the front of the chest, electrode #5 on the left side of the chest, electrode #9 on the back and electrode #13 on the right side of the chest |
| Data: | Data (zip format) |
| Image of Experimental Configuration: | |