Imaging electrode movement and conductivity changes in EIT

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Summary

- Electrical impedance tomography (EIT)
- Inverse problems
- Electrode movement in soft-field applications
- Methods of data acquisition
- Imaging algorithm with movement estimation
- Results
- Discussion

Electrical impedance tomography



EIT: lung ventilation

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Right: Lung ventilation imaging of normal human subject.

(Adler et al. 1994)

Left: Lung perfusion imaging using a conductive contrast in normal bovine subject. Images are compared with electron beam computerized tomography. (Frerichs *et al.* 2002)



EIT: encephalic imaging



A visual evoked response of a neonate. Activity is reported as due to changes in blood flow. (London EIT Group, 2006)

EIT numerical methods

- Finite Element Method (FEM) simulation software to model the forward and inverse problem
- EIDORS is *Electrical Impedance & Diffuse Optical Reconstruction Software* <u>http://www.eidors.org</u>
- forward: voltages from conductivity inverse: conductivity from voltages
- Avoid the inverse crime



EIT electrode movement



Left: Simulation of electrode movement of 1% medium diameter.

Right: Reconstruction of image assuming fixed electrode position.

• Since EIT is *ill-posed* we must struggle with extraneous solutions due to non-uniqueness (*i.e.* the system is underdetermined)

- We solve the inverse problem by *regularization* of the observed data using a priori information about the nature of the EIT system & our medium
 - A smoothness constraint to spatial variation of *conductivity* & neighboring electrode movement
 - Model noise as an additive white Gaussian process

EIT regularization algorithm

• The forward solution is modelled as a linear operator

$\mathbf{z} = \mathbf{J}\mathbf{x} {+} \mathbf{n}$

• Our reconstruction model quantifies the sensitivity of the voltage measurement due to conductivity and movement variations

$$\mathbf{J}_{i,j} = \frac{F_i(\mathbf{x}_j + \Delta \mathbf{x}_j)}{\Delta \mathbf{x}_j}$$

EIT regularization algorithm

- The inverse solution estimates using a onestep regularized inverse based on
 - \bullet noise model W
 - conductivity prior R_c
 - movement prior $\mathbf{R}_{\mathbf{m}}$

$$\mathbf{\hat{x}} = (\mathbf{J}^{t}\mathbf{W}\mathbf{J} + \lambda^{2}(\mathbf{R}_{c} + \mu^{2}\mathbf{R}_{m}))^{-1}\mathbf{J}^{t}\mathbf{z}$$

Forward simulation:

 576 element planar FEM with 2 contrasts of opposing conductivity
 Elliptical deformation of medium of 1% diameter (shown x20)
 AWGN of 20dB SNR

Standard reconstruction: 1. 256 element planar FEM rotated by 45 degrees 2. Hyperparameter $\lambda = 10^{-2}$



- Proposed reconstruction method:
- 1. Hyperparameters $\lambda = 10^{-2}$ and $\mu = 1$
- 2. Expected movement is 40%

Proposed reconstruction method:

- 1. Hyperparameters $\lambda = 10^{-2}$ and $\mu = 20$
- 2. Expected movement is 2%



Forward simulation: 1. 828 element 3D FEM 2. "Ellipse-twist" deformed 3. AWGN of 20dB SNR 4. Green plates are electrodes 5. Two contrasts of opposing conductivity



1st column: Forward simulation

2nd column: Standard reconstruction $\lambda = 3 \times 10^{-3}$

3rd column: *Proposed* $reconstruction_{\mu} = 20$



Discussion

- Benefits:
 - Estimating the electrode position resulted in a reduction of 70% of the artefact power for movements of 1% in 2D and 3D simulation
 - Results show reasonable estimates of actual electrode displacements (although not quantified)
 - Movement reconstructions have been tested on phantom data and show comparable results

Discussion

- Limitations:
 - Reconstruction requires manual adjustment of regularization hyperparameters μ
 - Noise priors used are simplistic and could be refined to represent true EIT noise
 - Electrode movements are modelled as translational only (no rotation or strain)